

# RuBi-Glutamate: two-photon and visible-light photoactivation of neurons and dendritic spines

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Rafael Yuste, Department of Biological Sciences, Columbia University, 1212 Amsterdam Avenue, Box 2435, New York, NY 10027, USA. e-mail: rafaelyuste@columbia.edu We describe neurobiological applications of RuBi-Glutamate, a novel caged-glutamate compound based on ruthenium photochemistry. RuBi-Glutamate can be excited with visible wavelengths and releases glutamate after one- or two-photon excitation. It has high quantum efficiency and can be used at low concentrations, partly avoiding the blockade of GABAergic transmission present with other caged compounds. Two-photon uncaging of RuBi-Glutamate has a high spatial resolution and generates excitatory responses in individual dendritic spines with physiological kinetics. With laser beam multiplexing, two-photon RuBi-Glutamate uncaging can also be used to depolarize and fire pyramidal neurons with single-cell resolution. RuBi-Glutamate therefore enables the photoactivation of neuronal dendrites and circuits with visible or two-photon light sources, achieving single cell, or even single spine, precision.

Keywords: uncaging, Ruthenium, bipyridine, RuBi-GABA

## **INTRODUCTION**

Caged compounds are becoming widely used in neuroscience because they enable the optical manipulation of neuronal circuits (Hess, 1999). Using photoreleasable neurotransmitters such as glutamate and GABA, one can activate or inhibit neuronal processes, single neurons, or groups of neurons (Ellis-Davies, 2005). Combining this with functional imaging provides a near ideal method of monitoring and controlling neuronal activity, allowing an entirely optical method for analysis of neural circuits (Nikolenko et al., 2007).

In particular, two-photon uncaging of glutamate, with its excellent spatial resolution, has been quite useful, due to the relatively high two-photon absorption cross sections of functionalized nitrobenzyl derivatives, such as 7-nitroindolinyl- and 4-methoxy-7-nitroindolinyl-amino (MNI) glutamate (Canepari et al., 2001; Matsuzaki et al., 2001). For example, two-photon uncaging of MNI-glutamate has been used successfully to functionally map synaptic receptors (Matsuzaki et al., 2001), activate individual spines (Araya et al., 2006; Carter and Sabatini, 2004; Gasparini and Magee, 2006; Matsuzaki et al., 2004; Sobczyk et al., 2005) and activate individual neurons (Nikolenko et al., 2007). In spite of its utility, MNI-glutamate needs to be applied to the tissue at relatively high (mM) concentrations for effective two-photon uncaging. Unfortunately, at these concentrations, MNI-glutamate, like other caged compounds, is a very effective antagonist of GABAergic transmission (see below for MNI glutamate; Maier et al., 2005; Molnar and Nadler, 2000 for other compounds). This can be a significant problem for its use in the study of neuronal circuits, as its application can lead to epileptiform events. Also, as it strongly blocks the GABAergic responses, it prevents the study of inhibitory network activity or connectivity.

To help circumvent this problem, we have exploited the flexibility of ruthenium chemistry, and have synthesized a novel series of

caged compounds, using ruthenium-bipyridine complexes (Zayat et al., 2003, 2005). Ruthenium is a transition metal, widely used due to its versatile chemistry. The polypyridines of ruthenium photorelease entire ligands in a heterolytic fashion, by means of a widely known mechanism in which the initial photoexcited state quickly evolves into a dissociative state, so the photorelease is therefore clean and fast (Zayat et al., 2003). We recently introduced a caged GABA compound ("RuBi-GABA") that can be used for optical inactivation of neurons and functional mapping of GABAergic currents (Rial Verde et al., 2008). Now we describe the biological characterization of a new caged glutamate compound, "RuBi-Glutamate", which can be photoreleased with one- or two-photon excitation and has less nonspecific effects than MNI glutamate. The chemical synthesis and photochemical characterization of RuBi-Glutamate is described elsewhere (Salierno et al., submitted). Although we expect that RuBi-Glutamate will be useful for one-photon visible uncaging experiments, in this report we mainly focus in its use for two-photon photostimulation, since there are already several adequate choices available for neuronal photostimulation with onephoton uncaging of glutamate (Callaway and Katz, 1993; Callaway and Yuste, 2002; Frick et al., 2001; Pettit et al., 1997; Shepherd et al., 2003; Wieboldt et al., 1994; Yoshimura et al., 2005).

#### **MATERIALS AND METHODS**

#### SLICE PREPARATION AND ELECTROPHYSIOLOGY

350 µm thick coronal slices from 14-day-old C57BL/6 mouse cortex were prepared using a Leica VT1000-S vibratome with a cutting solution containing (in mM): 27 NaHCO<sub>3</sub>, 1.5 NaH<sub>2</sub>PO<sub>4</sub>, 222 Sucrose, 2.6 KCl, 2 MgSO<sub>4</sub>, 2 CaCl<sub>2</sub>. Slices were incubated at 32°C in ACSF for 30 min and then kept at room temperature for at least 30 min before transferring them to the recording chamber. The recording chamber was bathed in ACSF (pH 7.4), also kept at room temperature and saturated with 95% O<sub>2</sub> and 5% CO<sub>2</sub>, containing (in mM): 126 NaCl, 3 KCl, 2 MgSO<sub>4</sub>, 2 CaCl<sub>2</sub>, 1 NaH<sub>2</sub>PO<sub>4</sub>, 26 NaHCO<sub>3</sub>, and 10 glucose.

Neurons were either held at their resting membrane potential (-65 mV), or at +40 mV, when both inhibitory and excitatory events were recorded. Whole-cell electrodes (4–7 M $\Omega$ ) were used. To establish whole-cell access the cells were illuminated with an oblique light and an IR-pass filter on the microscope field diaphragm, and visualized through a CCD camera (DAGE-MTI IR-1000) connected to a Sony PVM-137 black and white video monitor. All recordings, except those shown in Figures 2 and 3 were performed with intracellular solution (pH 7.25), containing (in mM): 135 K-methylsulfate, 10 KCl, 10 HEPES, 5 NaCl, 2.5 Mg-ATP, 0.3 Na-GTP, and 0.1 Alexa Fluor 594. Voltage-clamp recordings shown in Figures 2 and 3 were done with intracellular solution (pH 7.25), containing (in mM): 128 Cs-methanesulfonate, 10 HEPES, 2 MgCl<sub>2</sub>, 2 MgSO<sub>4</sub> 4 Na<sub>2</sub>-ATP, 0.4 Na-GTP, 10 Na<sub>2</sub>-phosphocreatine and 0.1 Alexa Fluor 594. Experiments were conducted at room temperature (22-25°C). We performed recordings from layer 2/3 and 5 pyramidal cells using MultiClamp 700B (Molecular Devices) amplifiers, and acquired the signals through a National Instruments PCI 6259 board using either custom software developed with LABView or Matlab. In a subset of experiments, electrical stimulations were performed using a bipolar electrode placed in layer 5. Repetitive stimuli were applied at a frequency of 0.2 Hz. CNQX  $(20 \,\mu\text{M})$  and APV  $(40 \,\mu\text{M})$  were routinely used while recording IPSCs, and TTX (2 µM) was added to the ACSF to isolate miniature synaptic currents.

Off-line analysis was conducted using Matlab, MiniAnalysis v6.0.7 or IGOR Pro with the Neuromatic v2.0 package. For consistency throughout the study, all measurements are expressed as mean  $\pm$  SEM. Statistical significance was assessed using Student's *t*-test and the non-parametric Mann–Whitney test when appropriate at the significance level (*p*) indicated.

## **RuBi-GLUTAMATE UNCAGING**

Images were acquired using a custom-made two-photon laser scanning microscope based on the Olympus FV-200 system (side-mounted to a BX50WI microscope with a 40×, 0.8NA, water immersion objective) and a Ti:sapphire laser (Chameleon Ultra II, Coherent, >3 W, 140 fs pulses, 80 MHz repetition rate). Fluorescence was detected with a photomultiplier tube (PMT: H7422-P40 Hamamatsu, Bridgewater, NJ, USA) connected to a signal amplifier (Signal Recovery AMETEK Advanced Measurement Technology, Wokingham, UK) whose output was connected to the Fluoview system. First, images of the soma were acquired with Fluoview software (XY scan mode with 1× to 10× digital zoom), at 850 nm using minimal power to prevent RuBi-Glutamate uncaging. As RuBi-Glutamate is light-sensitive, the computer screens and video monitor were covered with two layers of Rosco #27 medium red filters.

A somatic uncaging point was selected using custom software (Nikolenko et al., 2007), which triggered the uncaging pulse and controlled the pulse duration. Laser power was modulated by a Pockels cell (Quantum Technology, Lake Mary, FL, USA). For somatic stimulations, each uncaging target consisted of eight sub-targets, each of which was illuminated for 8 ms, giving a total duration of ~70 ms. The subtargets themselves were complex, consisting

of five very closely spaced beamlets created by multiplexing the laser beam with a diffractive optical element (DOE). The stimulations were repeated every 4 s. RuBi-Glutamate was added to the bath at 300  $\mu$ M concentration. The concentration chosen for two-photon experiments, 300  $\mu$ M, was the lowest concentration with which we were able to fire reliably using our stimulation protocol. While we performed other experiments with lower concentrations of RuBi-Glutamate (~150  $\mu$ M), neurons did not fire consistently (or sometimes not at all). One-photon experiments, were performed with 30  $\mu$ M the RuBi-Glutamate.

A Dynamax peristaltic pump (Ranin Instruments Inc., Woburn, MA, USA) was used to control bath perfusion to minimize total bath volume and re-circulate oxygenated media. Uncaging was performed with 800 nm light for two-photon experiments, and with 473 nm light for one-photon experiments.

To measure the lateral two-photon uncaging spatial resolution in single spines, the laser beam was positioned near the spine head (~0.2 µm from the spine head edge) and subsequently moved away from the spine head edge. We specifically decided not to uncage glutamate directly over the spine head to avoid damaging the spine membrane, which we know can be harmed by direct laser illumination. Instead, to prevent photodamage and trigger reliable glutamate responses without affecting the spine head, we directed the beam right next ( $\sim 0.2 \,\mu m$ ) from the spine head edge. With this stimulus protocol, we can reliably photostimulate spines for long periods of time without any appreciable photodamage. In addition, to measure the axial resolution of the RuBi-Glutamate uncaging responses, the laser beam was positioned next to the spine head and the uncaging responses were recorded at different focal planes (spaced every 0.8 µm). In these tests, 4 ms laser pulses at 2 s interval were used. To record desynchronized spontaneous miniature excitatory post-synaptic potentials (mEPSPs) from layer 5 neurons, we replaced extracellular calcium with strontium (Xu-Friedman and Regehr, 2000). Comparisons between mini-PSPs (mPSPs) or mini-PSCs (mPSCs) and photo-evoked responses are confounded by the spatial filtering. mPSPs or PSCs distributions are broad, stemming in part from the fact that the events are arising at many different spatial locations, each with a different cable-length filtering to the recording electrode, whereas in our photo-evoked responses the distances are much more uniform.

# **RESULTS**

# TWO-PHOTON UNCAGING OF RuBi-GLUTAMATE ACTIVATES GLUTAMATE RECEPTORS

RuBi-Glutamate (cis-[Ru(bpy)<sub>2</sub>(PMe<sub>3</sub>)GluH<sub>2</sub>](PF<sub>6</sub>)<sub>2</sub>, with bpy = 2,2'bipyridine and PMe<sub>3</sub> = trimethylphosphine) is a caged glutamate compound composed of a ruthenium center with six coordination positions, four of which are occupied by the two bidentate bipyiridines, the fifth by a trimethylphosphine and the sixth by a molecule of L-glutamate, coordinated through its amino group (**Figure 1A**). Upon absorption of one photon of visible light, or two near infrared photons, RuBi-Glutamate photocleaves within nanoseconds, and releases glutamate from the Ru-bipyridine core, with a quantum yield of ~0.13 at pH 7, and an extinction coefficient of >4,000 M<sup>-1</sup> cm<sup>-1</sup> at 473 nm (Salierno et al., submitted).

We first examined the ability of RuBi-Glutamate to activate glutamate receptors by performing whole-cell recordings from



(A) Structure of Ruthenium-bipyridine-trimethylphosphine-Glutamate (RuBi-Glutamate) and glutamate photorelease reaction. (B) Upper panel: Layer 2/3 pyramidal cell loaded with Alexa-594 and position of the multiplexed uncaging laser targets (eight subtargets) on the soma of the cell. Lower panel: Action potentials triggered by uncaging of RuBi-Glutamate (300 µM) in a layer 2/3

layer 2/3 pyramidal neurons in slices from mouse neocortex. Slices were bathed with a solution containing the caged form of RuBi-Glutamate and the laser beam was aimed toward the somata of the recorded neurons, uncaging glutamate, while simultaneously recording the membrane potential from the activated neuron, and monitoring the effect of the uncaging. Using this functional assay to probe two-photon uncaging, we explored several different excitation wavelengths and concentrations and found 800 nm to be optimal and 300 µM a sufficient RuBi-Glutamate concentration to generate reliable functional responses. For the one-photon studies mentioned here, we used 473 nm light and 30 µM RuBi-Glutamate, although because of the high absorption cross section for single photon excitation and the larger onephoton point spread function (PSF), we were also able to generate responses with concentrations as low as  $\sim 5 \,\mu$ M (data not shown). These wavelengths and concentrations agree with those expected by examining the photochemical properties of RuBi-Glutamate (Salierno et al., submitted), and also match those previously used in our work with other members of that family of RuBi-caged compounds, such as RuBi-GABA (Rial Verde et al., 2008).

pyramidal neuron. In this example, one action potential was evoked with a power on sample of 180 mW and two with 220 mW. (**C**) RuBi-Glutamate activates glutamate receptors. Adding APV (40  $\mu$ M) and CNOX (20  $\mu$ M) blocked the uncaging response. (**D**) Representative current–voltage plot of uncaging responses. Note how it reverses at +10 mV, indicating that the responses are mediated by glutamate receptors.

In pyramidal neurons, recorded under current clamp, twophoton uncaging of glutamate generated brief depolarizations, but with a single laser spot, the evoked depolarizations were too small to reliably cause the cell to fire action potentials. We therefore used a DOE to spatially multiplex the laser beam into five closely spaced beamlets, a strategy that we have previously introduced with MNI glutamate photostimulation (Nikolenko et al., 2007). This beamlet array was then directed onto eight subtargets on the cell (Figure 1B, upper panel), releasing more glutamate, generating stronger cellular responses leading to action potentials. Using this protocol, two-photon uncaging (on average, ~70 ms, 150–400 mW on the sample; n = 15 neurons) was able to reliably generate action potentials (Figure 1B, lower panel). Uncaging depolarizations ranged in amplitude from 1 to 20 mV and were effectively and reversibly blocked by bath application of the glutamate receptor antagonists APV/CNQX (Figure 1C; 40/20 µM respectively; 96.7  $\pm$  1.5% reduction in voltage, n = 6 neurons). In addition, in voltage-clamp conditions, RuBi-Glutamate uncaging generated inward currents that reversed at +10 mV, indicative of a glutamate receptor current (Figure 1D). These data confirmed that

the uncaging of RuBi-Glutamate activated glutamate receptors in cortical pyramidal neurons.

#### **EFFECT OF RuBi-GLUTAMATE ON SPONTANEOUS PSCs**

We then characterized the pharmacological effect of RuBi-Glutamate on synaptic receptors. As mentioned, the near complete blockade of inhibitory synaptic transmission by MNI-glutamate at concentrations useful for two-photon excitation (see below, **Figure 3**) prevents its clean use for circuit studies. To examine the effects from RuBi-Glutamate, we performed voltage-clamp recordings of spontaneous synaptic currents at different holding potentials, before and after bath application of RuBi-Glutamate. We performed these experiments with 300  $\mu$ M, the same concentration of RuBi-Glutamate that we used for two-photon uncaging. We also carried out experiments in the presence and absence of the sodium channel blocker TTX, in order to specifically test whether mPSCs were specifically affected by RuBi-Glutamate.

At resting membrane potential of -65 mV, bath application of 300 µM RuBi-Glutamate had no detectable effect on the average amplitude, frequency or rise time of spontaneous PSCs or of mPSCs in the presence of TTX (Figure 2A, n = 1,562 events from six control neurons, 1,775 from six neurons in the presence of RuBi-Glutamate). Since at -65 mV most PSCs are excitatory, these data indicated that bath applied RuBi-Glutamate had no significant effect on spontaneous excitatory PSCs (EPSCs). We then examined its potential effect on inhibitory PSCs (IPSCs), by performing similar experiments at +40 mV holding potential, a level at which both excitatory and inhibitory PSCs can be readily detected. At +40 mV, bath application of 300 µM RuBi-Glutamate produced a general trend of reducing the amplitude and frequency of spontaneous and miniature PSCs, with no apparent changes in the rise time of the events (Figure 2B). Although these effects were not statistically significant, in the presence of TTX, we did observe a significant reduction in PSCs frequency (p < 0.001, n = 6, t-test). This result, together with the lack of significant effect at -65 mV, close to the reversal potential of IPSCs, indicated a potential antagonistic effect of the caged form of RuBi-Glutamate on inhibitory currents.

#### EFFECT OF RuBi-GLUTAMATE ON EVOKED INHIBITORY TRANSMISSION

To directly examine if RuBi-Glutamate had an antagonistic effect on IPSCs we conducted a series of experiments in which we evoked inhibitory currents by stimulating the neuropil surrounding the recorded neuron with a stimulating electrode, while holding the neuron at +40 mV, in the presence of APV and CNQX (40/20  $\mu$ M, respectively) and thus better isolate IPSCs in the presence or absence of RuBi-Glutamate. The rationale of these experiments was to test whether RuBi-Glutamate blocked physiological synaptic GABAergic transmission, since our ultimate aim was to use twophoton uncaging of RuBi-Glutamate for circuit studies. Side-byside experiments were performed with MNI-glutamate in order to examine its effect on GABAergic currents. We tested the effects from MNI-Glutamate at both 300 µM, the concentration used in our RuBi-Glutamate uncaging experiments, and at the higher concentrations of MNI-Glutamate needed (>2.5 mM), in our experience, for effective two-photon MNI-glutamate uncaging.

In these experiments, the perfusion of 300  $\mu$ M RuBi-Glutamate generated a significant reduction of the peak amplitude of the evoked GABAergic IPSCs (**Figure 3**: 50.0 ± 6.0%, *n* = 7 cells, *p* < 0.001). Perfusion of MNI-glutamate at the same concentrations (300  $\mu$ M) generated an even more pronounced decrease in evoked IPSCs (**Figure 3B**; 83.0 ± 3.0%, *n* = 4, *p* < 0.001). At 2.5 mM, the concentration needed for effective two-photon uncaging, MNI-glutamate completely blocked the evoked response (**Figure 3**: 97.0 ± 2.0%, *n* = 6, *p* < 0.001).

We concluded that, although 300  $\mu$ M RuBi-Glutamate has a significant antagonist effect on endogenous GABAergic currents, this effect (close to 50%) is smaller compared with that of MNI glutamate (~80% at 300  $\mu$ M, ~100% at the effective concentration of 2.5 mM). The differences between the 50% reduction observed in these RuBi-Glutamate experiments vs. the smaller reduction observed in the +40 mV recordings of spontaneous miniature potentials in TTX (**Figure 2**) may be partly due to the fact that at +40 mV one records a mixture of EPSCs and IPSCs.

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We then tested the use of two-photon uncaging of RuBi-Glutamate for activating dendritic spines, one of the most useful applications of two-photon glutamate uncaging (Araya et al., 2006; Carter and Sabatini, 2004; Gasparini and Magee, 2006; Matsuzaki et al., 2004; Sobczyk et al., 2005). For these experiments, we performed wholecell recordings from pyramidal neurons and filled them with Alexa 594 to optimally visualize their dendritic spines. We then bathed the slice in RuBi-Glutamate (300 µM) and directed a pulsed laser at the neuropil adjacent to a chosen spine (Figures 4A,B). With 4 ms laser pulses, we triggered reliable depolarizations in the neuron (see traces in Figures 4C,D). These responses were similar in amplitude to events recorded after two-photon uncaging of MNIglutamate (see Table 1). However, the RuBi-Glutamate generated neuronal responses had a rate of rise nearly twice as fast as those generated from uncaging MNI-glutamate (p < 0.001, n = 65 RuBi-Glutamate uncaging events from four spines vs. n = 127 MNI-glutamate uncaging events from nine spines). In addition, 10-90% rise times and 37% decay time kinetics were faster then those observed with uncaging of MNI-glutamate (p = 0.001 and p < 0.001, respectively, Table 1), and more closely resemble the kinetics of spontaneous mEPSP (Table 1, see Materials and Methods for detection of mEPSPs).

In these single spine experiments, we also explored the spatial resolution of the uncaging responses, by monitoring the evoked depolarization while changing the position of the laser with respect to the dendritic spine. Moving the uncaging spot perpendicular to the spine (i.e., in the XY plane) resulted in a strong decrease in the amplitude of the uncaging response (~80% reduction with the beam 1.3  $\mu$ m away from the spine, **Figure 4C**; n = 7 spines and 2 neurons). In the axial (Z) direction, a small change in position, 0.8  $\mu$ m, also resulted in a strongly diminished voltage response (**Figures 4D,E**; 71% average reduction; n = 30 uncaging events, n = 2 neurons). These results are consistent with the small local uncaging volume defined by the two-photon PSF, and are similar to measurements obtained with two-photon uncaging of



MNI-glutamate (Araya et al., 2006). Thus, two-photon uncaging of RuBi-Glutamate has a spatial resolution that approximates the dimension of a typical dendritic spine, and therefore can be used to selectively activate individual spines.

# RuBi-GLUTAMATE UNCAGING CAN ACTIVATE INDIVIDUAL NEURONS

Finally, we tested the potential use of RuBi-Glutamate for the optical photostimulation of neurons. These types of experiments, in which one uncages glutamate to elicit action potentials from a desired



FIGURE 3 | Effect of RuBi-Glutamate and MNI-glutamate on inhibitory transmission. (A) Voltage-clamp responses of a pyramidal neuron to extracellular electrical stimulation. An external bipolar stimulation electrode was used to evoke responses while clamping the neuron at +40 mV and in presence of APV (40 μM) and CNQX (20 μM) in the ACSF to isolate the GABA currents.

Here we show examples of IPSCs evoked in control conditions, and the diminution of their amplitude after adding either RuBi-Glutamate (300  $\mu$ M, left part) or MNI-Glutamate (300  $\mu$ M or 2.5 mM, right part) to the bath. **(B)** Histogram showing averages of the inhibition of GABA current in presence of RuBi-Glutamate or MNI-Glutamate. \*\*p < 0.01, \*\*\*p < 0.001.



FIGURE 4 | Use of RuBi-Glutamate uncaging to optically activate dendritic spines. (A) Layer 2/3 neuron loaded with Alexa-594 to detect dendritic spines. (B) Higher resolution image of a dendritic spine selected for uncaging. Red dots indicate the sites of uncaging. (C) Plot of the XY spatial resolution of uncaging from the spine shown in (B) (Inset, traces corresponded to averages of 15 uncaging potentials at the different locations [1–4; red dots

in (B)]. (D) Spatial axial resolution of uncaging. Z-stack of images from the stimulated spine. Traces corresponded to averages of 15 uncaging potentials of its corresponding image stack. Red dots indicate the site of laser beam parking, not the actual size of the beam profile. (E) Plot of the axial resolution at the three different locations showed in (D).

	Amplitude (mV)	Rate of rise (mV/ms)	10–90% rise time (ms)	Decay time (ms)
RuBi–Glu	1.20 ± 0.09 ( <i>n</i> = 65)	0.092 ± 0.01 ( <i>n</i> = 65)	13.98 ± 1.13 ( <i>n</i> = 65)	23.11 ± 1.79 ( <i>n</i> = 59)
MNI–Glu	0.92 ± 0.03 (n = 127)	0.04 ± 0.002 (n = 127)	19.08 ± 1.24 ( <i>n</i> = 127)	53.43 ± 4.24 (n = 114)
Sr <sup>2+</sup> -mEPSPs	$0.55 \pm 0.006 \ (n = 1,317)$	$0.06 \pm 0.001$ ( $n = 1,316$ )	$8.20 \pm 0.09 (n = 1,316)$	$16.06 \pm 0.21 \ (n = 1,217)$

 Table 1 Effect of RuBi-Glutamate on spontaneous synaptic currents.
 Pairwise comparisons between MNI-Glutamate vs. RuBi-Glutamate, MNI-Glutamate vs. mEPSP and RuBi-Glutamate vs. mEPSPs were statistically significant for all four variables with p < 0.001.
 Values expressed as mean  $\pm$  SEM.



neuronal target, have been very useful for mapping the synaptic inputs in slices (Callaway and Katz, 1993; Shepherd et al., 2003; Yoshimura et al., 2005). Moreover, with two-photon excitation, these inputs maps can be built with single-cell precision (Nikolenko et al., 2007).

These experiments were performed by recording from pyramidal neurons with whole-cell electrodes and directed the uncaging laser onto the soma of the cells, in slices bathed with 300  $\mu$ M RuBi-Glutamate (**Figure 5A**). As previously mentioned, we used eight subtargets and a DOE to spatially multiplex the laser beam (**Figure 5B**). With this protocol we reliably generated action potentials in the recorded neuron ( $90.0 \pm 2.6\%$  action potential occurrence, ~70 ms uncaging pulses, n = 11 cells; **Figure 5**).

We characterized the effective spatial resolution of our multispot uncaging protocol by moving the spatiotemporally multiplexed laser pattern away from the somata of the cell (Figure 5B), and measuring the amplitude of subthreshold postsynaptic depolarizations and the probability of suprathreshold events as a function of the distance of the closest target from the cell edge. For subthreshold events, in the XY plane, we measured a strong decrease in the amplitude of the uncaging response, with a minimal response at 10  $\mu$ m away from the soma (normalized amplitude: 0.10  $\pm$  0.01, n = 8 neurons; Figure 5C). Movements in the Z plane resulted in a smaller modulation of the response amplitude (normalized amplitude:  $0.19 \pm 0.02$  at 30 µm, n = 5 neurons; Figure 5C). Because the multiple beamlets and target pattern are dispersed in space, the subthreshold event spatial resolution was understandably worse than that that is obtained with single laser spots (Figure 4). Nevertheless, for suprathreshold events, we observed a strong decrease of the occurrence of evoked action potentials as the uncaging targets were moved only 2 µm from the edge of the soma in XY plane (3.0  $\pm$  2.8% of occurrence of an action potential, n = 7neurons) and 5  $\mu$ m above the soma in Z plane (10.0  $\pm$  7.6%, n = 4neurons; Figure 5C). In these experiments, we avoided uncaging near any prominent dendritic processes. However, the same stimulation conditions used to generate an action potential while targeting the soma, only generate subthreshold responses when intentionally (or accidentally) targeting the dendrites.

We also explored the use of one-photon RuBi-Glutamate uncaging in similar experiments, using 30  $\mu$ M RuBi-Glutamate and a single laser spot, aimed at the center of the somata. With 1 ms laser pulses, one-photon RuBi-Glutamate uncaging generated reliable depolarizations in the cell. The spatial resolution of this response was different in the XY and Z planes, with minimal responses at 15 (normalized amplitude: 0.14 ± 0.03, *n* = 4 neurons) and 40  $\mu$ m (normalized amplitude: 0.20 ± 0.03, *n* = 3 neurons), respectively.

These experiments demonstrated that RuBi-Glutamate can be used, in both one- and two-photon mode, for reliable photostimulation of neurons in brain slices. In particular, the spatial resolution of two-photon DOE uncaging appears adequate for studies with single-cell precision.

## DISCUSSION

Here we introduce the use of RuBi-Glutamate as a novel chemical tool for the photoactivation of individual dendritic spines and cortical neurons in circuits. In the past, glutamate uncaging has been successfully used to map circuits with one-photon excitation (Bureau et al., 2004; Callaway and Katz, 1993; Shepherd et al., 2003; Yoshimura et al., 2005). The synthesis of MNI-glutamate (Canepari et al., 2001; Matsuzaki et al., 2001) enabled the two-photon photoactivation of spines (Araya et al., 2006; Matsuzaki et al., 2004) and neurons (Nikolenko et al., 2007), although the unspecific effects of MNI-glutamate on synaptic receptors have prevented its use for two-photon studies of inhibitory circuits.

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RuBi-Glutamate has a number of desirable properties, such as a relatively high absorption cross section in the visible (blue) and a high quantum efficiency of uncaging (Salierno et al., submitted). This combination allows RuBi-Glutamate to be used at lower concentrations than MNI-glutamate, lessening the blockade of GABAergic responses. The ability of the RuBi-compounds to absorb and uncage with visible light, compared to other caged glutamate compounds, which require UV excitation, is also significant, as blue light has higher penetration and lower toxicity for living tissue. Although we have only performed a cursory exploration of the use of RuBi-Glutamate for one-photon uncaging, we should mention that it has some useful features that other users may find it potentially interesting for one-photon experiments. Specifically, we have effectively uncaged glutamate with visible light from a variety of sources including standard mercury/xenon lamps, LED sources, or even laser pointers and flashlights, something that makes the instrumentation needed for glutamate uncaging experiments quite accessible and inexpensive. Also inexpensive glass optics instead of UV-transparent quartz can be used for uncaging of RuBi-Glutamate.

Perhaps more importantly, the red-shifted single photon spectrum leads to a red-shifted two-photon uncaging peak (800 nm for RuBi-Glutamate vs. 725 with MNI-Glutamate). In addition to the deeper penetration into tissue, 800 nm is near the peak of the maximum power output for the Ti-Sapphire lasers commonly used for two-photon experiments, which means more power is available to uncage glutamate at multiple sites simultaneously, an important consideration for future experiments aimed at probing complex neural circuit dynamics (Nikolenko et al., 2008).

Our initial experience with RuBi-Glutamate has been positive and we report a number of advantages that could make it widely used. It is water-soluble and does not have any strong pharmacological effects at the concentrations explored for effective one- or two-photon uncaging. Although at higher concentrations ( $300 \mu$ M) it significantly reduces GABAergic responses, it does not block them, so it could allow for the mapping of inhibitory circuits, and the stimulation of dendritic spines in regimes where inhibition is still partly engaged, resulting in more physiological experiments. This, combined with the decreased phototoxicity and increased penetration depth of the longer wavelengths required for uncaging RuBi-Glutamate compared with the nitrobenzyl and nitroindolinyl glutamate derivatives, could make *in vivo* uncaging experiments feasible.

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**Conflict of Interest Statement:** The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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